

# Real-Time Motion Correction in Magnetic Resonance Spectroscopy: AI solution inspired by fundamental science

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## Abstract

Magnetic Resonance Spectroscopy (MRS) is a powerful non-invasive tool for metabolic tissue analysis but is often degraded by patient motion, limiting clinical utility. The RECENTRE project (REal-time motion CorrEctioN in magneTic Resonance) presents an AI-driven, real-time motion correction pipeline based on optimized GRU networks, inspired by tagging and fast-trigger algorithms from high-energy physics. Models evaluated on held-out test sets achieve good predictive performance ( $R^2 > 0.87$ ) and overall positive framewise displacement (FD) gains. These results demonstrate feasibility for prospective scanner integration; future work will complete in-vivo validation.

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## Contents

<sup>3</sup> <b>1</b>	<b>Introduction</b>	<b>2</b>
<sup>4</sup> <b>2</b>	<b>Neural Network and Framewise Displacement approach</b>	<b>2</b>
<sup>5</sup> <b>3</b>	<b>Results</b>	<b>3</b>

6	4 Conclusions	4
7	References	5
8		
9		

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## 10 1 Introduction

11 Magnetic Resonance (MR) is a well-established, non-invasive modality for the study of tissue  
12 structure and function. Magnetic Resonance Spectroscopy (MRS) [1] extends MR to metabolic  
13 and biochemical assessment, with potential clinical applications. However, patient motion re-  
14 mains a critical obstacle: even modest displacements produce spectral distortions, baseline  
15 shifts and loss of quantification that reduce reproducibility and limit diagnostic value. The  
16 RECENTRE project proposes a real-time motion correction [2] [3] [4] pathway for MRS based  
17 on compact deep recurrent networks. The design is inspired by algorithmic techniques from  
18 high-energy physics, such as tagging and fast-triggering [5], which enable low-latency deci-  
19 sions on streaming data. Training and evaluation emphasise two complementary goals. First,  
20 the model must accurately [6] predict motion-related parameters that can be used for prospec-  
21 tive adjustment during the acquisition. Second, the training objective explicitly favours reduc-  
22 tions in framewise displacement while preserving spectral fidelity.

## 23 2 Neural Network and Framewise Displacement approach

24 Recurrent neural networks (RNNs) are naturally suited for modeling sequential data, as they  
25 capture temporal dependencies across consecutive observations. Among their variants, Gated  
26 Recurrent Units (GRUs) provide an effective balance between modeling capacity and com-  
27 putational efficiency, achieving performance comparable to long short-term memory (LSTM)  
28 networks with fewer parameters and reduced training time. Within the RECENTRE project,  
29 a GRU-based architecture was therefore adopted to predict motion corrections directly from  
30 short temporal sequences of MR acquisitions.

### 31 Dataset

32 The data used for training were obtained from the Human Connectome Project (HCP) [7]. A  
33 total of 1113 subjects were scanned on Siemens 3T MRI systems with a repetition time (TR)  
34 of 720 ms and an echo time (TE) of 33.1 ms. Three acquisition types have been included  
35 in this work, differing in the number of frames per sequence: Resting State (1200 frames),  
36 Working Memory (316 frames), and Language (405 frames). The motion parameters used as  
37 input to the network consist of three translations and three rotations, extracted through rigid  
38 realignment during post-processing of the MRI data. As illustrated in Fig. 1, the network input  
39 was formed by 7 sequences of two data points each (14 in total), then the model predicts the  
40 following 15th point.

### 41 Framewise displacement gain

42 Framewise displacement (*FD*) was employed as a subject-specific index of motion, providing  
43 a scalar measure of head movement at each time point.  
44 *FD* was computed both from the ground-truth (Eq. 1) and the predicted motion parameters

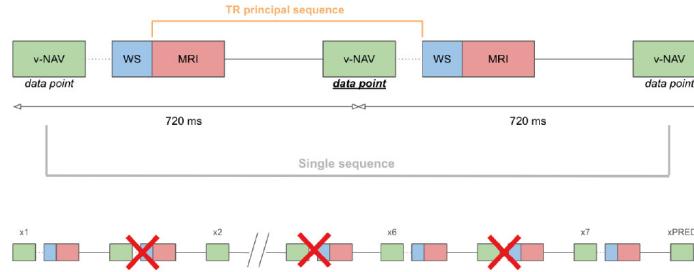


Figure 1: Each input sample consists of 7 sequences, each covering two consecutive acquisition points (for a total of 14 time points). The model is trained to predict the subsequent 15th point.

45 (Eq. 2).

$$FD_{\text{total}} = \sum_{i=1}^3 |T_{i,t} - T_{i,t+1}| + \frac{50\pi}{180} \sum_{i=1}^3 |R_{i,t} - R_{i,t+1}| \quad (1)$$

$$FD_{\text{predicted}} = \sum_{i=1}^3 |\hat{T}_{i,t+1} - T_{i,t+1}| + \frac{50\pi}{180} \sum_{i=1}^3 |\hat{R}_{i,t+1} - R_{i,t+1}| \quad (2)$$

46 where  $T_i$  denote the translational motion parameters (in mm) and  $R_i$  the rotational motion  
 47 parameters (in rad), with the index  $i = 1, 2, 3$  corresponding to the three spatial directions.  
 48 The quantities  $\hat{T}_i$  and  $\hat{R}_i$  denote the corresponding predicted parameters. The  $FD$  gain was  
 49 then defined as:

$$FD_{\text{gain}} = \frac{FD_{\text{total}} - FD_{\text{predicted}}}{FD_{\text{total}}}. \quad (3)$$

50 A positive  $FD_{\text{gain}}$  indicates an improvement, i.e. reduced motion relative to the original se-  
 51 quence.

## 52 Neural network model and training objective

53 The adopted model is composed of a GRU layer with hidden size 128, followed by normal-  
 54 ization, non-linear activations and two fully connected layers. The total number of trainable  
 55 parameters is approximately 270k. The network outputs the predicted motion parameters to-  
 56 gether with their associated uncertainty estimates. Training was performed with the Adam  
 57 optimizer and early stopping based on validation performance. The loss function combined a  
 58 probabilistic negative log-likelihood (NLL) term with a term ( $\beta FD_{\text{gain}}$ ) that promote positive  
 59  $FD$  gains and effective motion reduction on motion reduction:

$$\mathcal{L} = \text{NLL} - \beta FD_{\text{gain}} \quad \beta = 0.1 \quad (4)$$

60 This design enforces both predictive accuracy and effective reduction of head motion. The  
 61 corresponding training and validation loss curves for the three acquisition types are reported  
 62 in Fig. 2.

## 63 3 Results

64 Results were obtained on the held-out test set across the three acquisition types (Resting State,  
 65 Working Memory, and Language), as described in Section 2.  
 66 Training curves (Fig. 2) demonstrate stable convergence of the loss across all acquisition types.  
 67 No significant overfitting was observed.

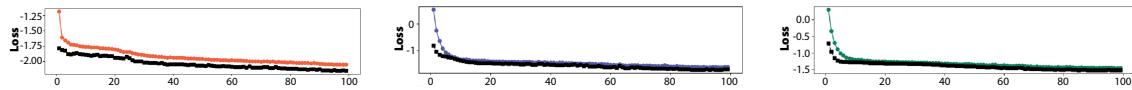


Figure 2: Training and validation loss curves for the three acquisition types: on the left Resting state set, in the middle Working memory set and on the right Language set.

68 Prediction accuracy was evaluated by comparing the predicted motion parameters with the  
 69 corresponding ground-truth values, scatter plots show good agreement, as illustrated in Fig. 3.  
 70 Quantitative performance was assessed using the coefficient of determination ( $R^2$ ), computed  
 71 between predicted and ground-truth parameters on the test sets. Across all tasks,  $R^2$  values  
 72 consistently exceeded 0.87, indicating reliable predictive performance.

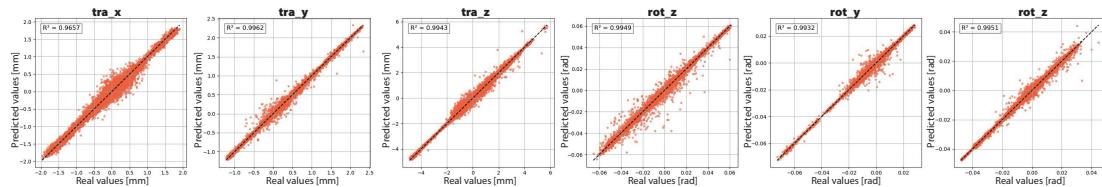


Figure 3: Predicted vs. true motion parameters on the test set for the Resting State acquisition. The figure reports the six estimated motion parameters, namely the three rotational displacements (in rad) and the three rotational angles (in mm).

73 The effectiveness of the network in reducing apparent motion was quantified using the FD  
 74 gain metric (see Eq. (3)). Positive FD gains were consistently observed across all acquisition  
 75 (Fig. 4), demonstrating improved motion estimates. Results were comparable among Resting  
 76 State, Working Memory, and Language tasks.

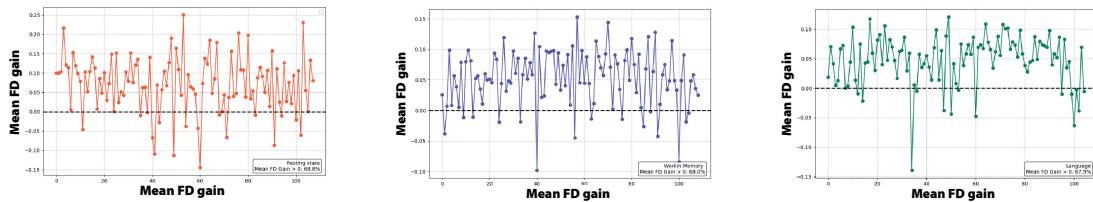


Figure 4: Mean FD gain per patient (average over all predictions). Negative FD gains indicate that the network sometimes slightly overestimates motion.

## 77 4 Conclusions

78 The GRU-based predictor achieves high predictive accuracy ( $R^2 > 0.87$ ) across evaluated di-  
 79 mensions, capturing both large and subtle motion patterns. FD-gain analysis shows mostly  
 80 positive values, reflecting a net reduction of estimated motion for the majority of patients, with  
 81 only occasional slight overestimation. The GRU network will be integrated into the Siemens  
 82 syngo MR MAGNETOM workflow, where the Siemens Image Calculation Environment (ICE)  
 83 will use the predicted roto-translation parameters for motion-corrected image reconstruction.  
 84 The model will run on the Siemens Framework for Image Reconstruction Environment (FIRE)  
 85 with deployment on the Siemens MARS workstation, leveraging on-board GPUs to accelerate  
 86 prediction. Validation will be performed on in-vivo data acquired with the Siemens 3T Prisma  
 87 scanner at IRCCS Santa Lucia in Rome.

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## 91 References

92 [1] M. G. Saleh, R. A. E. Edden, L. Chang and T. Ernst, *Motion correction in magnetic resonance*  
93 *spectroscopy*, Magn. Reson. Med. **84**, 2312 (2020), doi:[10.1002/mrm.28287](https://doi.org/10.1002/mrm.28287).

94 [2] O. C. Andronesi, P. K. Bhattacharyya, W. Bogner and et al., *Motion correction methods for mrs: experts' consensus recommendations*, NMR Biomed. **34**, e4364 (2020),  
95 doi:[10.1002/nbm.4364](https://doi.org/10.1002/nbm.4364).

96 [3] B. Keating, W. Deng, J. C. Roddey, N. White, A. Dale, V. A. Stenger and T. Ernst, *Prospective*  
97 *motion correction for single-voxel 1h mr spectroscopy*, Magn. Reson. Med. **64**, 672 (2010),  
98 doi:[10.1002/mrm.22448](https://doi.org/10.1002/mrm.22448).

99 [4] A. Marsman, E. T. Lind, M. Petersen, V. Andersen and V. O. Boer, *Prospective frequency and*  
100 *motion correction for edited 1h magnetic resonance spectroscopy*, Neuroimage **233**, 117922  
101 (2021), doi:[10.1016/j.neuroimage.2021.117922](https://doi.org/10.1016/j.neuroimage.2021.117922).

102 [5] S. Giagu, *Fast and resource-efficient deep neural network on fpga for the phase-ii level-0 muon barrel trigger of the atlas experiment*, In EPJ Web Conf., vol. 245, p. 01021,  
103 doi:[10.1051/epjconf/202024501021](https://doi.org/10.1051/epjconf/202024501021) (2020).

104 [6] D. Tamada, *Review: Noise and artifact reduction for mri using deep learning*, arXiv:2002.12889 [physics], Available at: <https://arxiv.org/abs/2002.12889> (2020).

105 [7] W.-M. H. C. P. Consortium, *WU-Minn HCP 1200 Subjects Release: Reference Manual*,  
106 Updated April 2018; available at [https://humanconnectome.org/storage/app/media/documentation/s1200/HCP\\_S1200\\_Release\\_Reference\\_Manual.pdf](https://humanconnectome.org/storage/app/media/documentation/s1200/HCP_S1200_Release_Reference_Manual.pdf) (2018).